This scientific commentary refers to ‘Individual brain structure and modelling predict seizure propagation’, by Proix et al. (doi:10.1093/brain/awx004).

Epilepsy continues to be a debilitating disease, which often cannot be fully controlled through medication. In such cases, patients may be referred for surgery to remove the piece of brain that appears to be the source of the problem—the epileptogenic zone (EZ). Unfortunately, surgical treatment is not always successful, partly because the methods for identifying the epileptogenic zone and its influence on the surrounding propagation zone (PZ) are still ad hoc. Formulation of more complex treatment plans is limited by our ignorance of the processes of brain function and dysfunction. Tools for brain imaging and manipulation—MRI, functional MRI, diffusion MRI, EEG, SEEG, MEG, brain stimulation and others—are improving rapidly, and further tools are expected in the near future as a result of major new funding initiatives. The problem: ‘big data’—little theory. In this issue of Brain, Proix, Bartolomei, Guye and Jirsa take a bite out of our theoretical ignorance by providing personalized computer models of patients with epilepsy to begin to explain each patient’s individual seizure genesis and spread (Proix et al., 2017).

William Lennox, epileptology pioneer, metaphorized epilepsy as a river—‘the river of epilepsy’ (Fig. 1) (Lennox and Lennox, 1960). This expressed the notion that epilepsy is a complex set of diseases—the epilepsies—with multiple possible causes that can combine in myriad ways to produce seizures. Experimentalists generally work at the lower scales, the contributory tributary level, assessing predisposing genetics, ion channel anomalies, responses to brain trauma, etc. Many computational modellers also work from this perspective, attempting to put together simulations that include the details of ion channels and synaptic connectivity (Lytton, 2008). The clinician, however, is faced with the river—the clinical syndromes that represent the many little pieces put together. Proix et al. have taken on the challenge of modelling this end-result, the river, by looking at final common pathways that govern the mathematical dynamics of seizure genesis and seizure spread. An excellent brief description of dynamical systems theory in the context of neurobiological applications is found in Breakspear and Jirsa (2007).

Fifteen drug-resistant patients with epileptogenic zones defined by SEEG were modelled. The personalized models were developed using the Virtual Brain (thevirtualbrain.org), a dynamical systems theory simulation tool developed by one of the authors (Sanz-Leon et al., 2013). Dynamical systems theory concerns itself with the understanding of coupled differential equations, describing how parts of a system interact over time through positive and negative feedback. For this study, each individual brain area was defined by an ‘Epileptor’ (Jirsa et al., 2014). Each epileptor has five state variables whose differential equations are given by Equation 4 in Proix et al. (2017). These state variables provide fast seizure-like oscillations ($x_1, y_1$), slower spike-and-wave activity ($x_2, y_2$) and ‘permittivity’ ($z$). $x_1 + x_2$, summed together, resemble a local field potential or SEEG. Epileptor nodes are localized based on MRI-aided individualized anatomical parcellation. Over 100 epileptor nodes (subscript $i$ in Equation 4 in Proix et al.) are connected to form the complete brain network model (BNM) to simulate seizure activity in that patient’s brain.

Each epileptor node has a baseline excitability parameter, $x_{0,i}$ (note that the $x_{1,i}$ is a state variable; $x_{0,i}$ is a parameter). A group of nodes with high excitability can become spontaneously active—these make up the epileptogenic zone. Other nodes have lower excitability but can be driven into seizure—these are potentially part of the propagation zone (Fig. 2). Full simulations of the BNM were complemented by analysis involving dimensional reduction and linearization. Individual epileptors are linked together by connectivity parameters $K_{ij}$, undirected weighted graph edges determined from that patient’s white matter tractography measured from diffusion MRI. The $K_{ij}$ connectivity parameters drive permissivity for a node using the sum of differences between that node’s $x_{1,i}$ and those of each input area.

The patient’s BNM will generate likely scenarios (hypotheses) about patterns of seizure spread. The
patterns of activation of the propagation zones in sets of simulations are then compared to both the clinical estimation of the propagation zone and to the propagation zone pattern observed on SEEG during a seizure. Unfortunately, as is common in efforts to formalize clinical diagnosis and decision-making, comparison is limited due to lack of a ground truth. The clinical assessment is hampered by precisely the missing theoretical understanding that this project attempts to alleviate. SEEG data are partial due to limited coverage and sampling. Note that there is no single model but rather a family of models that generate a set of hypotheses about origin and spread. For example, the location of the epileptogenic zone is given, rather than being estimated from the data. The BNM can then be used to validate this hypothesis about the location of the epileptogenic zone based on the accuracy of the predicted propagation zone.

This ‘Epileptor 0.1’ software cannot yet be used directly in the clinic. Instead, we look to the future. Personalized data acquisition of cortical and subcortical parcellation, tractography, activity, and susceptibility will be more readily, rapidly, inexpensively, and non-invasively obtained. The Virtual Brain BNM will improve in precision and accuracy. These BNMs will then provide reasonably accurate, reasonably precise models of epilepsy spread (although never a single correct model—brain modelling is more akin to weather prediction than it is to the kinematics of satellites). Evidence from BNMs can be
Glossary of dynamical system terms

The Hodgkin-Huxley (HH) equations and the solar system will be used as examples to illustrate some of the terminology.

**Analytic solution:** A solution to a set of differential equations that defines each state variable as a function in time. These solutions can generally not be found for linked ODE systems of three or more state variables.

**Bifurcation:** A dramatic change in dynamic pattern with change in one parameter. The classic case from neurobiology is the bifurcation with change in I (input current) in the Hodgkin-Huxley equations. This bifurcation takes the stable resting membrane potential (a point attractor) and causes an oscillation (the spiking) along a limit cycle.

**Bistability:** The ability of a system to show two (or more for multistability) different dynamical patterns without any change in parameters. The ability of a system to show either seizure activity or normal physiological activity will in some cases be due to a situation of bistability across a separatrix.

**Chaos:** Phenomenology seen in some dynamical systems which show high-dimension strange attractors and sensitivity to initial conditions. Chaotic systems are interesting as their trajectories appear to be random but are in fact deterministic.

**Dimensional reduction:** A high dimensional system such as Hodgkin-Huxley or the epileptor cannot be directly visualized. Therefore, one attempts to simplify these systems by various methods—for example, noting where one state variable closely follows another; this will allow one to create a lower-dimensional system with similar dynamics.

**Dimensionality:** The number of dimensions of the state space or of a subspace to which trajectories are restricted (called a manifold). The dimensionality of the Hodgkin-Huxley equations is 4; for a pendulum 2: instantaneous position, instantaneous momentum. The dimensionality of the single epileptor is 5 while the group of n epileptors will have dimensionality 5n.

**Equilibrium point:** A solution to a dynamical system that does not change with time. An equilibrium can be unstable as for example the proverbial pencil balanced on its point.

**Initial conditions:** The starting values of the state variables. Along with the parameters and the ODEs, the initial conditions are part of the full description of a specific dynamical system.

**Limit cycle attractor:** A stable recurring trajectory in state space, an orbit. A system perturbed slightly from a limit cycle attractor will return to it.

**Numerical solution:** An approximate solution to a set of differential equations obtained through simulation on a computer. These simulations are done by approximating \(dx/dt\) based on using a small but finite time step \(\Delta t\) in place of the infinitesimal \(dt\). This allows calculation of a \(\Delta x\) at each time step, which is used to update the current value of \(x\).

**Ordinary differential equations (ODEs):** Equations that provide values for \(dx/dt\), the change in state variable \(x\), with infinitesimal time \(dt\). When the right-hand side of the equation depends on other state variables (coupled ODEs), these quantities interact with each other in complicated positive and negative feedback loops. ODEs can be distinguished from partial differential equations (PDEs) such as those describing reaction-diffusion. Note that \(\dot{x}\) is an alternative notation for \(dx/dt\).

**Parameterization:** The setting-up and the organization of parameters. The functional forms that define the right hand side of the ODEs form part of the parameterization.

**Parameters:** Fixed values in the system. For the solar system, a parameter would be the force of gravity. For the Hodgkin-Huxley equations, parameters include \(C_m\), \(g\), I (capacitance, leak conductance, input current).

**Point attractor:** An equilibrium location in state space towards which all trajectories flow.

**Point repeller:** Opposite of an attractorall trajectories move away from this point in state space.

**Separatrix:** A boundary that separates two different regions of state space, which feature different dynamical patterns. In the context of the epileptor there is a separatrix that keeps apart the region of epileptic dynamics from the region of physiological dynamics.

**State space:** An abstract space with dimensions corresponding to the number of state variables. If there are three state variables \(x, y, z\) then the position of the entire system at a given time can be represented as a single point in 3D space.

**State variable:** A representative of a quantity that is determined by a differential equation. State variables will thereby change in time. The state variables for Hodgkin-Huxley are \(v, m, h, n\): voltage, \(Na^+\) channel activation, \(Na^+\) channel inactivation, \(K^+\) channel activation.

**Trajectory:** The path of a state variable through state space. If the state space is only 2 or 3 dimensions this can be depicted graphically. Otherwise trajectories of each individual state variable can be depicted as line graphs of values on the \(y\)-axis with time on the \(x\)-axis. Note that the usual trajectory representations for orbits of planets in the solar system only show half of the state space as the state variables for the solar system include momentum as well as position for each planet.

Acronyms

**BNM:** Brain network model

**dMRI:** Diffusion MRI – traces white matter tracts

**ECoG:** Electrographicography

**EEG:** Electroencephalography

**EZ:** Epileptogenic zone

**fMRI:** Functional MRI – measures activity via local oxygenation

**MEG:** Magnetoencephalography

**MRI:** Magnetic resonance imaging – measures anatomy

**PZ:** Propagation zone

**SEEG:** Stereotactic EEG – local field potential from implanted electrodes

**VB:** The Virtual Brain
taken together with other models—genomic predictive models, detailed simulation models, statistical models—along with clinical judgement, to determine a treatment plan. The clinician will run BNMs with perturbations that correspond to possible surgical options, including removal of all or parts of the epileptogenic zone, partial removal of parts of the propagation zone, tractotomies dividing parts of the epileptogenic zone or dividing epileptogenic zone from propagation zone, etc. This will provide plans for cure based on surgeries (or non-invasive ablations) that cannot currently be proposed.

How can the Virtual Brain help us understand the real one? Brain oscillations are thought to furnish the underpinnings of perception, motivation, thought and consciousness via mechanisms of firing synchronies creating representations. The Virtual Brain recreates some of these dynamics and can potentially explain how these oscillations permit area-to-area synchronies, as well as how these dynamics are disturbed to create seizures and to produce various movement disorders. The four activity state variables $x_1, y_1, x_2, y_2$ can be grossly mapped onto the activity of underlying excitatory-inhibitory population interactions that produce network effects (Wilson and Cowan, 1972). The slow permittivity state variable $z$ may be a reflection of changes in extracellular ionic concentrations, oxidative state, or metabolism. In a prior paper, the authors explicitly showed how these measures in whole ex vivo immature mouse hippocampus would map onto $z$ (Jirsa et al., 2014). Overall, however, the difficulty in mapping dynamic phenomenology remains a limitation of this type of phenomenological model, which portrays the river (Fig. 1) without reference to the tributaries. Meanwhile, multiscale mechanistic models, built from the bottom-up, have the opposite failing—providing a view of the details but not providing any way to understand the overall functional mechanisms of the brain. Filling in ‘the missing middle’ of mesoscopic modelling to connect top and bottom remains a major challenge for the future.

Finally, personalized modelling is an important step forward for personalized medicine. Personalized medicine and precision medicine emerged from the human genome project. It has now become apparent that big data does not equal big knowledge and big clinical plans. Theory now emerges at multiple scales to begin to fill these gaps.

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References

Penumbral salvage and thrombolysis outcome: a drop of brain, a week of life

This scientific commentary refers to ‘Perfusion computed tomography in patients with stroke thrombolysis’, by Kawano et al. (doi:10.1093/brain/aww338).

In ischaemic stroke, a thrombus abruptly occludes a cerebral artery, reducing blood flow to a focal region of the brain. While a small group of cells experiences complete loss of blood supply and dies within the first few minutes, a much larger region experiences more moderate, and variable, reduction in blood flow that tissues can withstand for tens of minutes to a few hours. If early reperfusion is not achieved, the zone of irreversibly infarcted tissue (the ‘ischaemic core’) expands over the next several hours, incorporating more and more of the tissues that were initially ailing but salvageable (the ‘penumbra’). Saving the penum-